

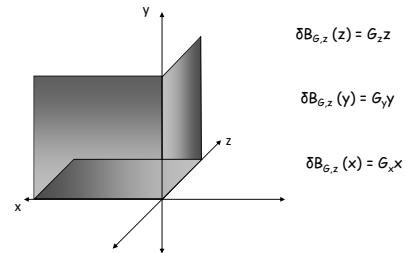
FYS-KJM 4740

MR-teori og medisinsk diagnostikk

Kap 2 (forts) Bildedannelse & K-space

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Magnetfelt-gradient



Fase-effekt av gradient (f.eks i y-retn):

$$\alpha(\mathbf{r}, t) = -\gamma \int_0^t G_y(t) \cdot \mathbf{r} \cdot d\tau$$

Transversal magnetisering er da gitt ved (fra Bloch's likn - ser bort fra T2-relaks):

$$M_{xy} = M_T(\mathbf{r}, t) = M_T(\mathbf{r}, 0) \cdot \exp \left(-j \gamma \int_0^t G_y(t) \mathbf{r} d\tau \right)$$

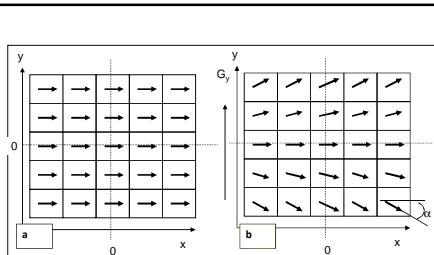
MR-signal = integral av transv. magnetisering over posisjon:

$$M_T(t) \propto S(t) \propto \iiint \rho(\mathbf{r}) \exp \left(-j \gamma \int_0^t G_y(t) \mathbf{r} d\tau \right) d\mathbf{r}$$

NB: Fourier transform

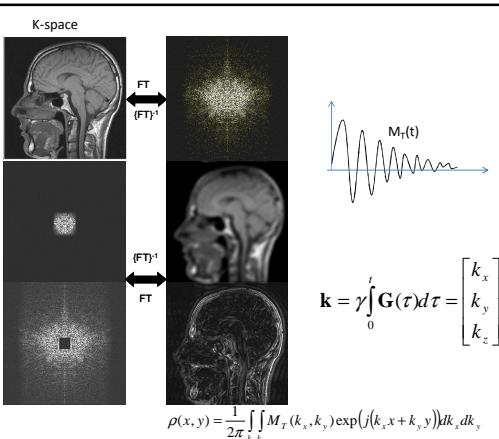
$$F(k) = \iiint_R f(\mathbf{r}) \exp(-jk\mathbf{r}) d\mathbf{r}$$

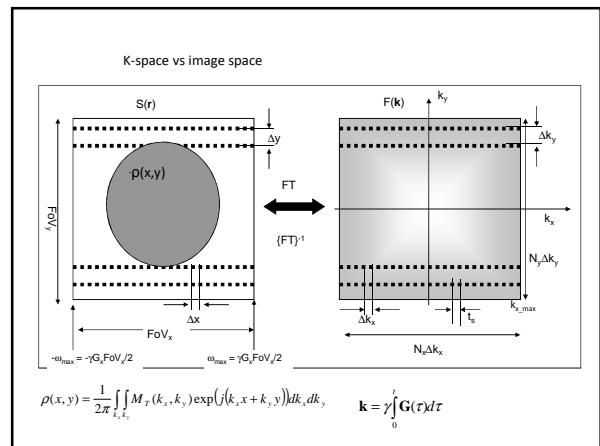
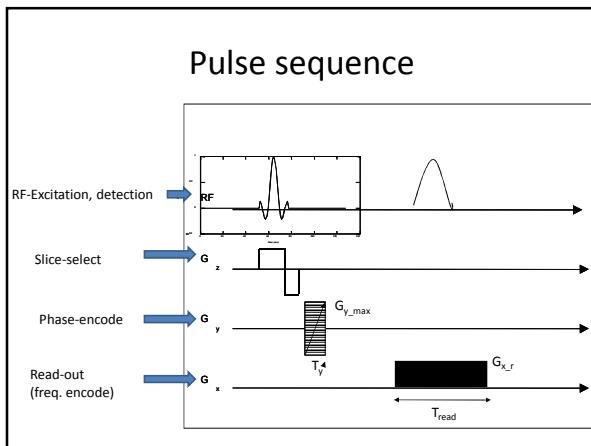
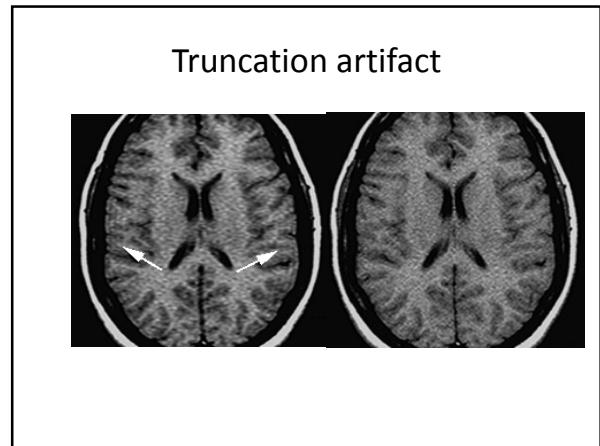
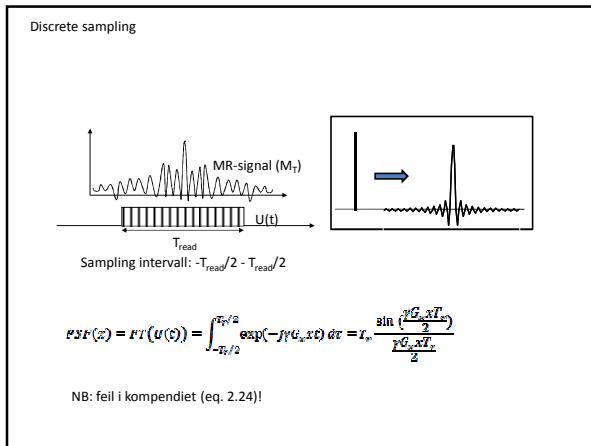
$$S(t) \propto \iiint_R \rho(\mathbf{r}) \exp \left(-j \gamma \int_0^t G_y(t) \mathbf{r} d\tau \right) d\mathbf{r}$$



The phase angle of the transverse magnetization vector before (a) and after (b) the application of a magnetic field gradient in the y-direction.

$$\mathbf{k} = \gamma \int_0^t \mathbf{G}(\tau) d\tau = \begin{bmatrix} k_x \\ k_y \\ k_z \end{bmatrix} \quad M_T(t) = \iint_{slice} \rho(\mathbf{r}) \cdot \exp(-j\mathbf{k} \cdot \mathbf{r}) d\mathbf{r}$$





K-space egenskaper

Resolution (x):	Maximum frequency in read-out (x) direction
$\Delta x = \frac{2\pi}{\gamma G_x N_x t_s}$	$\pm \omega_{\text{max}} = \pm \gamma G_x F_o V_x / 2$
Field of view (x):	Min sampling rate (x):
$\lambda_{x,\text{max}} = \frac{2\pi}{k_{x,\text{min}}} = \frac{2\pi}{\gamma G_x t_s} = F_o V_x$	$1/t_s \geq \gamma G_x F_o V_x / 2\pi$
Field of view (y):	'Sampling rate' (y):
$\lambda_{y,\text{max}} = F_o V_y = \frac{\pi N_y}{\gamma G_{y,\text{max}} T_y}$	$N_y = \gamma G_{y,\text{max}} T_y F_o V_y$

