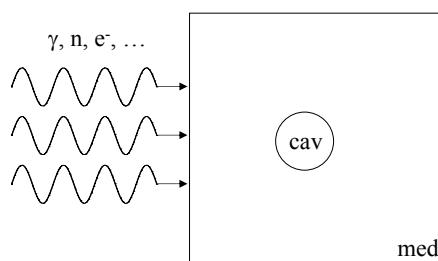


Cavity theory and Interface dosimetry

Eirik Malinen

 RIKSHOSPITALET RADIUMHOSPITALET

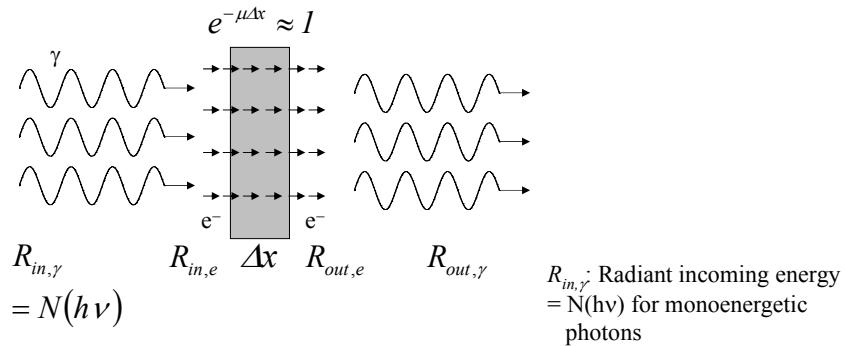
Cavity



- Cavity theory, narrow sense: convert “dose to detector” to “dose to medium”
- Cavity theory, broad sense: dose distribution in inhomogeneous media

 RIKSHOSPITALET RADIUMHOSPITALET

Absorbed dose in γ irradiated thin foil, CPE



Energy transferred:

$$\begin{aligned}\varepsilon_{tr} &= R_{in,\gamma} + R_{in,e} - R_{out,\gamma} - R_{out,e} = R_{in,\gamma} - R_{out,\gamma} \\ &= N(h\nu)\mu_{tr}\Delta x\end{aligned}$$



RIKSHOSPITALET RADIUMHOSPITALET

Absorbed dose in γ irradiated thin foil, CPE

Absorbed dose (no brehmsstrahlung)

$$D = K = \frac{\varepsilon_{tr}}{m} = \frac{N(h\nu)\mu_{tr}\Delta x}{m} = \frac{\Psi A \mu_{tr}\Delta x}{\rho A \Delta x} = \Psi \left(\frac{\mu_{tr}}{\rho} \right)$$

$$\mu_{tr} = \mu \frac{\bar{T}}{h\nu}$$

If brehmsstrahlung:

$$D = K_c = \Psi \left(\frac{\mu_{en}}{\rho} \right)$$



RIKSHOSPITALET RADIUMHOSPITALET

Energy loss from electrons

- Stopping power:

$$S = \frac{dT}{dx} = S_{col} + S_{rad} = \rho n \int_{E_{min}}^{E_{max}} E \left(\frac{d\sigma_{tot}}{dE} \right) dE$$

- Collision stopping power: S_{col}

$$S_{col} = \rho n \int_{E_{min}}^{E_{max}} E \left(\frac{d\sigma_{col}}{dE} \right) dE$$

n : number of atomic electrons per gram

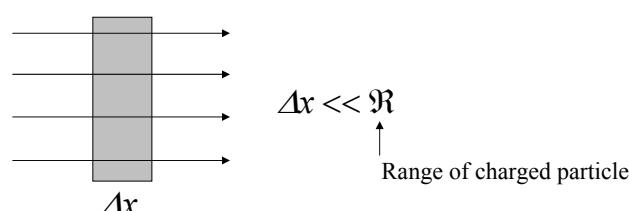
- Restricted stopping power: L_Δ

$$L_\Delta = \rho n \int_{E_{min}}^{\Delta} E \left(\frac{d\sigma_{col}}{dE} \right) dE$$



RIKSHOSPITALET RADIUMHOSPITALET

Absorbed dose in thin foil, electrons



Energy loss $\langle \Delta T \rangle \rightarrow$ energy imparted ε ?

→ **Brehmsstrahlung, δ rays, path lengthening**

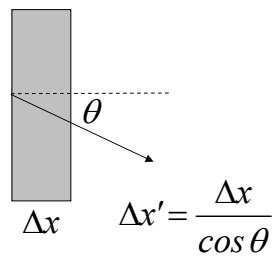
Brehmsstrahlung: S_{rad}



RIKSHOSPITALET RADIUMHOSPITALET

Path lengthening due to multiple scattering

$$\overline{\cos(\theta)} = \cos\left(\sqrt{\rho\Delta x} \frac{d\overline{\theta^2}}{dx}\right)$$



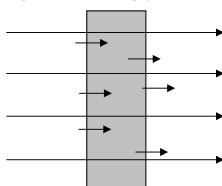
Scattering power: $\frac{d\overline{\theta^2}}{dx}$



RIKSHOSPITALET RADIUMHOSPITALET

δ rays

- Energetic, secondary electrons
 - Significant range compared to foil thickness
 - Results from high energy transfers (included in S_{col})



Maximum energy transfer:

$$E_{max} = 2m_e c^2 \frac{\beta}{1-\beta^2}$$

Heavy ions



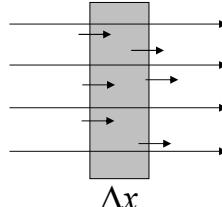
RIKSHOSPITALET RADIUMHOSPITALET

δ rays

Energy imparted for charged particles:

$$\varepsilon = R_{in,p} + R_{in,\delta} - R_{out,p} - R_{out,\delta}$$

↑
primary



δ particle equilibrium

$$R_{in,\delta} = R_{out,\delta} \Rightarrow \varepsilon = R_{in,p} - R_{out,p}$$

δPE requirements: homogeneous medium and $\mathfrak{R}_\delta \ll \mathfrak{R}_p$

δPE always present under CPE



RIKSHOSPITALET RADIUMHOSPITALET

δ rays

- Since β is low for heavy charged particles in the MeV-region, E_{max} is low
- $\beta=0.1$ (e.g. 38 MeV α-particles) gives $E_{max}=10$ keV
- Range of 10 keV electrons in water: 2.5 μm
- →δ-electrons deposit their energy locally, and δ-equilibrium may often be present
- Range of 1 MeV electrons: 0.5 cm
- →δ-equilibrium may not be obtained for high energy electron beam



RIKSHOSPITALET RADIUMHOSPITALET

Absorbed dose

$$D = \frac{\varepsilon}{m}$$

- Under δ PE (foil sandwiched, short \mathfrak{R}_δ), no path lengthening, no brehmstrahlung:

$$\varepsilon = R_{in,p} - R_{out,p} = \Delta R_p = NS\Delta x$$

$$\Rightarrow D = \frac{NS\Delta x}{\rho V} = \frac{NS\Delta x}{\rho A \Delta x} = \frac{N S}{A \rho} , \quad \Phi = \frac{N}{A}$$

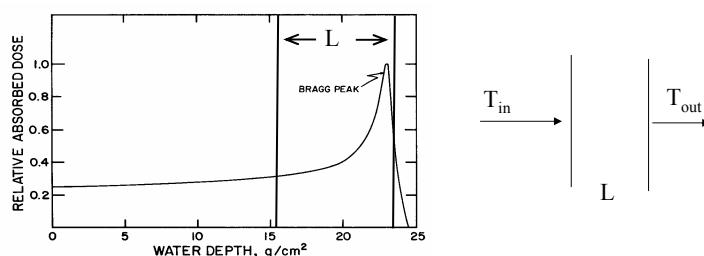
$$D = \Phi \left(\frac{S}{\rho} \right)$$

Fluence of primary electrons



RIKSHOSPITALET RADIUMHOSPITALET

Absorbed dose, thick foil, heavy particles



- The average dose may be found by:

- Calculating the residual range: $\mathfrak{R}_{res} = \mathfrak{R}_{in} - L$
- Find the energy T_{out} corresponding to \mathfrak{R}_{res}
- Imparted energy is: $\Delta T = T_{in} - T_{out}$
- Dose: $D = \frac{N \Delta T}{m} = \Phi \frac{\Delta T}{\rho L}$



RIKSHOSPITALET RADIUMHOSPITALET

Foil placed in vacuum

δ rays with $T > \Delta$ lost from foil (δ PE absent):

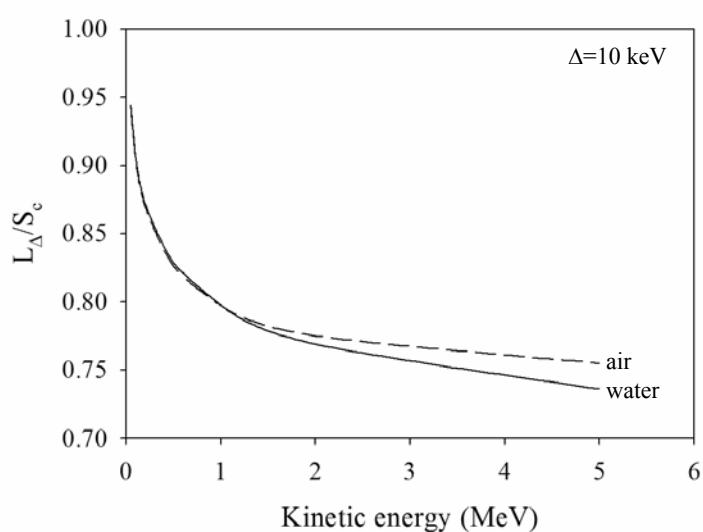
$$\varepsilon = R_{in,p} - R_{out,p} - R_{out,\delta} = N \left[\rho n \int_{E_{min}}^{\Delta} E \frac{d\sigma}{dE} dE \right]$$

$$D = \Phi \left(\frac{L_\Delta}{\rho} \right)$$



RIKSHOSPITALET RADIUMHOSPITALET

L_Δ



RIKSHOSPITALET RADIUMHOSPITALET

Spectrum of charged particles, δ PE present

$\Phi_T dT$: number of primary electrons cm⁻² in [T, T+dT]

Minimum energy: 0

Maximum energy: T_{max}

$$\Rightarrow dD = \Phi_T dT \left(\frac{S}{\rho} \right) \Rightarrow D = \int_0^{T_{\max}} \Phi_T dT \left(\frac{S}{\rho} \right)$$

$$D = \int_0^{T_{\max}} \Phi_T \left(\frac{S}{\rho} \right) dT$$



RIKSHOSPITALET RADIUMHOSPITALET

Partial δ PE

Electron beams: constant fluence of secondary, low energy electrons with T < Δ

Energetic secondary electrons added to total fluence:

$$D = \int_{\Delta}^{T_{\max}} \Phi_T^{p+\delta} \left(\frac{L_{\Delta}}{\rho} \right) dT$$

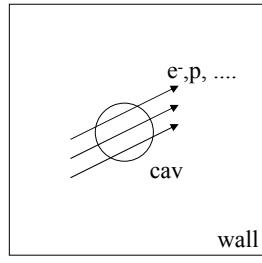
$$\Phi_T^{p+\delta} ?$$

Particles either assigned to radiation field or to energy imparted



RIKSHOSPITALET RADIUMHOSPITALET

Bragg-Gray cavity theory


$$D_{cav} = \Phi \left(\frac{S}{\rho} \right)_{cav}$$
$$D_{wall} = \Phi \left(\frac{S}{\rho} \right)_{wall}$$
$$\Rightarrow \frac{D_{cav}}{D_{wall}} = \left(\frac{S}{\rho} \right)_{wall}^{cav}$$

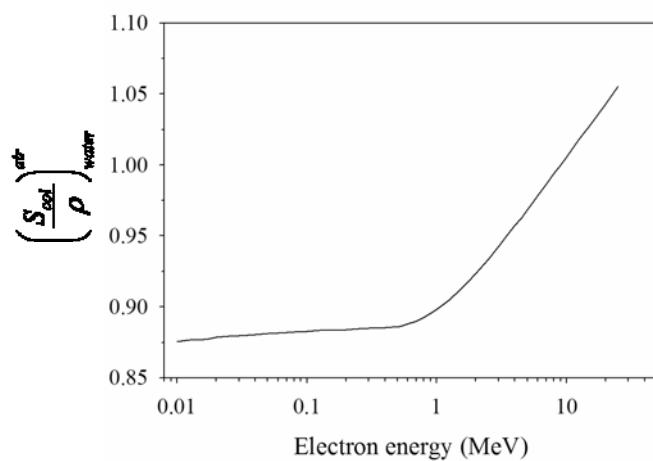
B-G conditions:

1. Charged particle fluence is not perturbed by cavity
2. Absorbed dose entirely due to charged particles



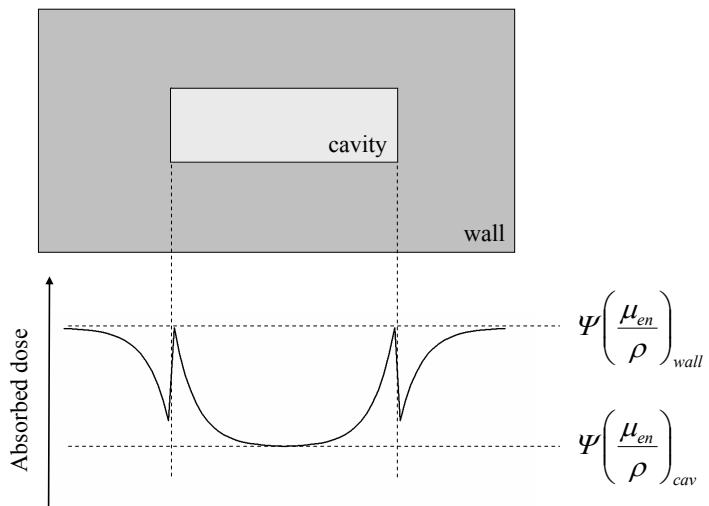
RIKSHOSPITALET RADIUMHOSPITALET

Bragg-Gray cavity theory



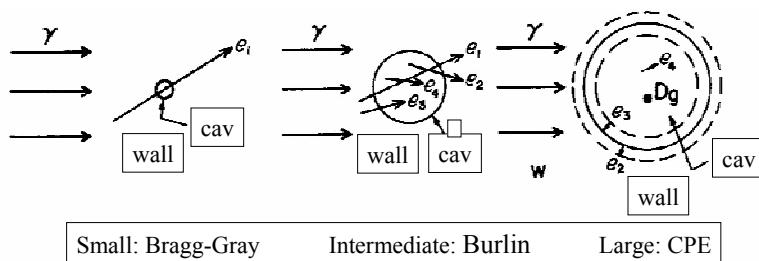
RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory



RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory



RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory

Cavity with dimensions << electron range: B-G theory:

$$\frac{D_{cav}}{D_{wall}} \approx \left(\frac{S}{\rho} \right)_{wall}^{cav}$$

Cavity with dimensions >> electron range: CPE-theory:

$$\frac{D_{cav}}{D_{wall}} = \left(\frac{\mu_{en}}{\rho} \right)_{wall}^{cav}$$



RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory

General theory for intermediate sized cavities:

$$\frac{D_{cav}}{D_{wall}} = d \left(\frac{S}{\rho} \right)_{wall}^{cav} + (1-d) \left(\frac{\mu_{en}}{\rho} \right)_{wall}^{cav}$$

d: average attenuation of electrons generated in the wall crossing the cavity

$$d = \frac{\int_0^L e^{-\beta x} dx}{\int_0^L dx} = \frac{1 - e^{-\beta L}}{\beta L} \Rightarrow 1 - d = \frac{\beta L + e^{-\beta L} - 1}{\beta L}$$



RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory

β : effective electron attenuation coefficient

Empirical expression:

$$e^{-\beta t_{max}} \approx 0.04$$

t_{max} : depth at which 1 % of electrons can travel

$$t_{max}/\mathfrak{R}_{CSDA} \approx 0.9 \text{ low } Z$$

$$t_{max}/\mathfrak{R}_{CSDA} \approx 0.8 \text{ intermediate } Z$$

$$t_{max}/\mathfrak{R}_{CSDA} \approx 0.7 \text{ high } Z$$



RIKSHOSPITALET RADIUMHOSPITALET

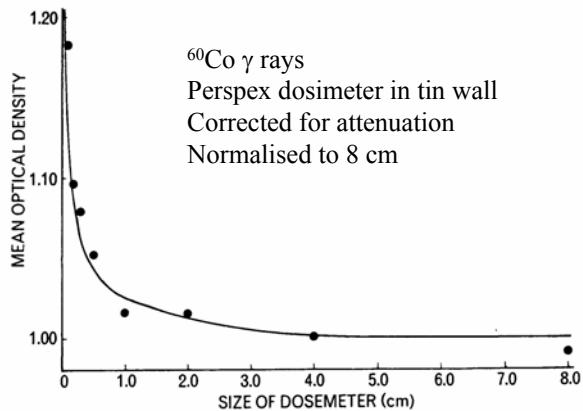
Burlin cavity theory - assumptions

- Wall and cavity homogenous
- No significant γ attenuation
- CPE exists
- Spectrum of δ rays equal in wall and cavity
- Electrons generated in wall are exponentially attenuated within cavity
- Electrons generated in cavity increase exponentially



RIKSHOSPITALET RADIUMHOSPITALET

Burlin cavity theory – experiment vs theory



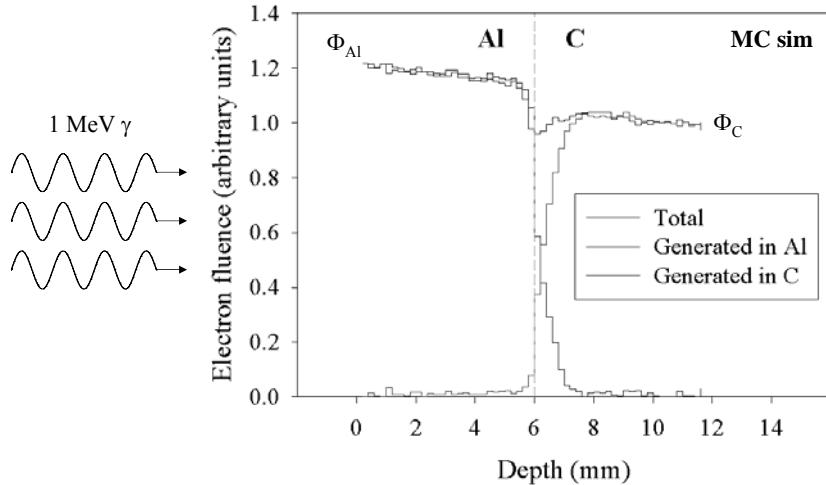
RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry



RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry



RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry

Total equilibrium fluence, secondary electrons, CPE:

$$\Phi = n_0 \mathfrak{R}_{CSDA}$$

Remember that

$$n_0 \bar{T}^{CPE} = \Psi \frac{\mu_{en}}{\rho} = N h \nu \frac{\mu_{en}}{\rho} \approx n_0 \frac{\mu_{en}}{\mu} h \nu$$

$$\Rightarrow n_0 = N \frac{\mu}{\rho}$$



RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry

Therefore, fluence ratio, medium 1 and 2 becomes:

$$\frac{\Phi_1}{\Phi_2} = \left(\frac{\mu}{\rho} \right)_2^1 \left(\mathfrak{R}_{CSDA} \right)_2^1$$

1 MeV γ rays:

$$\bar{T} = 0.45 \text{ MeV} , \left(\frac{\mu}{\rho} \right)_C = 0.064 \text{ cm}^{-1} , \left(\frac{\mu}{\rho} \right)_{Al} = 0.061 \text{ cm}^{-1}$$

$$\mathfrak{R}_C = 0.186 \text{ g/cm}^2 , \quad \mathfrak{R}_{Al} = 0.211 \text{ MeV cm}^2/\text{g}$$

$\Phi_{Al}/\Phi_C \approx 1.10$, against 1.14 for MC

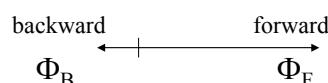


RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry

At the interface, transition from Φ_1 to Φ_2

Simplistic vector representation:

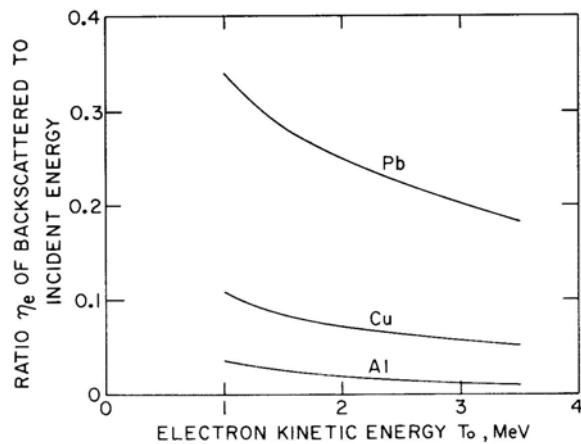


Forward/backward ratio depend on medium



RIKSHOSPITALET RADIUMHOSPITALET

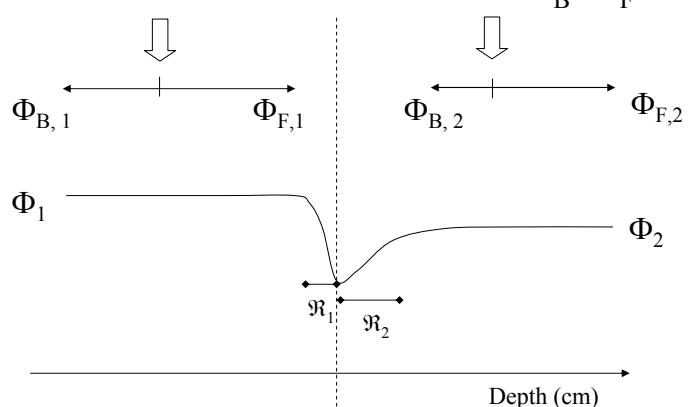
Backscatter ratio



RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry

Simplistic considerations – total fluence $\Phi_B + \Phi_F$

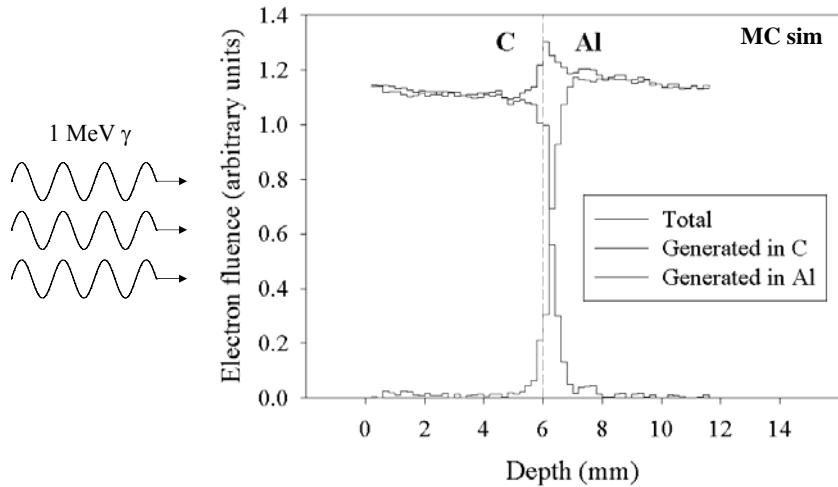


At interface, $\Phi_{tot} \approx \Phi_{B,2} + \Phi_{F,1}$



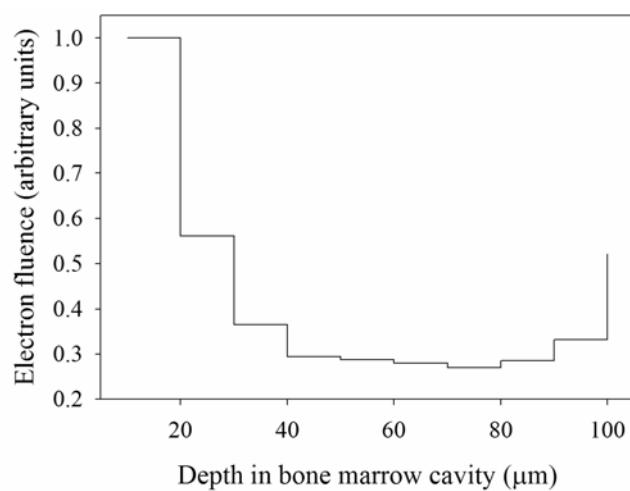
RIKSHOSPITALET RADIUMHOSPITALET

Interface dosimetry



RIKSHOSPITALET RADIUMHOSPITALET

X ray dose to bone marrow, Monte Carlo



RIKSHOSPITALET RADIUMHOSPITALET