



Dosimeter model

• Consider a dosimeter consisting of a wall and a sensitive volume:

v v w

• Wall: source of secondary electrons; shields V from electrons originating outside wall; mechanical protection of V; container (if V gas or liquid); may filter the beam.

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Dosimetry - recap • With cavity theory, the dosimeter energy response may be determined • If photon irradiation + CPE: $D = K_c = \Psi\left(\frac{\mu_{en}}{\rho}\right)$ • If charged particle irradiation: $D = \Phi\left(\frac{S}{\rho}\right)$ • Theory of Burlin for intermediate-sized cavities

Dosimetry characteristics

- An *absolute* dosimeter directly provides a measure of absorbed dose without requiring calibration
- Examples: calorimetric dosimeters, ferrous sulfate dosimeters, *ionization chambers*
- A *relative* dosimeter provides a reading that is proportional to absorbed dose, and requires calibration
- Examples: thermoluminescence dosimeters, diodes, film dosimeters, EPR dosimeters

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Accuracy

- Accuracy reflects the proximity of the estimate to the true value
- Reflects all systematic error contributions that influence the reading
- Example: calibration error



Precision

- Precision, or reproducibility, reflects fluctuations in in instrument, ambient conditions, stochastic nature of radiation fields
- Precision in single measurement can be estimated from a series of dosimeter readings {r_i}:

$$\sigma = \sqrt{\frac{1}{n-1} \left(\sum_{i=1}^{n} (r_i - \bar{r})^2 \right)}$$

• Precision in mean estimate: $\sigma = \sqrt{\frac{1}{n(n-1)} \left(\sum_{i=1}^{n} (r_i - \bar{r})^2\right)}$

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Dosimeter limitations

- A sensitive dosimeter is characterized by a high dr/dD
- A constant sensitivity (dr/dD = const) means a linear dose response
- A dosimeter may give a background reading r₀
- If r₀ is small, the lower detection limit is given by the dosimeter readout system
- The upper detection limit depends both on the readout system and the dosimeter material

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Ionometry

- Ionometry: the science of measuring ionizations
- Number of ionizations proportional to dose







Ionometry

- High voltage over inner and outer electrode
- Air is ionized; electrons are liberated
- Electrons collected at the positive electrode
- Induced current
- The number of charges produced is counted by an electrometer, which also provides the voltage
- Number of charges proportional to dose to air

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Exposure

- Exposure, X : number of charges Q (either positive or negative) prodused in a gass of mass m:
 - $X = \frac{dQ}{dm}$
- Number of charges per mass proprtional to dose: $X \propto D_{air}$
- The quantity relating X to D_{air} is the mean energy per ion pair, \overline{W}

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Dose to air, D_{air}

- For air, $\overline{W/e}$ is 33.97 J/C
- The dose to air:

$$D_{air} = \frac{N\overline{T_0}}{m} = \frac{Q}{m} \left(\frac{W}{e}\right)_{air} = X \left(\frac{W}{e}\right)_{air}$$

 Thus, by measuring the number of charges produced per mass unit of air, D_{air} may be determined – indepedent of the radiation quality (W/e is close to being constant for all electron- and photon energies)

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Dose to air, D_{air} 2

• If CPE is present in the ion chamber, the dose following photon irradiation is:

$$D_{air} \stackrel{CPE}{=} K_{c, air} = \Psi\left(\frac{\mu_{en}}{\rho}\right)_{air} = X\left(\frac{W}{e}\right)_{air}$$

• The exposure is thus:

$$\mathbf{X} \stackrel{\text{CPE}}{=} \Psi \! \left(\frac{\boldsymbol{\mu}_{\text{en}}}{\boldsymbol{\rho}} \right)_{\! air} \! \left(\frac{\overline{\mathbf{W}}}{e} \right)_{\! air}^{\! -1}$$

(If the primary field is charged particles, Bragg-Gray theory may be used: $D_{air} = \Phi\left(\frac{dT}{\rho dx}\right)_{air}$





Exposure, examples 3
 If the same exposure is resulting from 100 MeV protons, what is the corresponding energy fluence? For protons, Bragg-Gray theory is used: D_{ait} = Φ(dT/ρdx)_{ait} = X(W/e)_{ait} The proton energy is virtually constant over the
cavity: $\Rightarrow \Psi = \Phi T_{0} \Rightarrow \frac{\Psi}{T_{0}} = X \left(\frac{\overline{W}}{e}\right)_{air} \left(\frac{dT}{\rho dx}\right)_{air}^{-1}$
$\Rightarrow \Psi = XT_0 \left(\frac{\overline{W}}{e}\right)_{air} \left(\frac{dT}{\rho dx}\right)_{air}^{-1}$
$= \frac{0.064 \text{ C/kg} \times 100 \text{ MeV} \times 33.97 \text{ J/C}}{6.43 \text{ MeV cm}^2 / g} = \frac{0.034 \text{ J/cm}^2}{2000 \text{ J/cm}^2}$
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Practical ion chamber dosimetry 2

• For a given dose to water, D_w, an ion chamber reading M is obtained. Thus:

 $D_{w} \propto M \iff D_{w} = MN_{D,w}$

• The calibration factor is:

$$N_{\rm D,w} = \frac{D_{\rm w}}{M}$$

- Thus, the dose may be determined without using W/e, μ_{en}/ρ etc

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Practical ion chamber dosimetry 4

- However, the calibration factor is (weakly) dependent on the radiation type and energy, due to differences in absorption properties between water and air.
- Keep in mind (μ_{en}/ρ) the (dT/ ρ dx)-ratios, and that M is proportional to $D_{air}!$
- Usually, the chamber is calibrated in a well defined field, e.g. ⁶⁰Co γ-rays (average energy 1.25 MeV)
- Corrections of the calibration factor, k_Q, is thus introduced for other energies (radiation "qualities", e.g. 15 MV X-rays)

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